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U.O.C. Oftalmologia  
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**AngioPlex**

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**Performance e successi degli OCT/Angio-OCT**



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# Foreword: 25 Years of Optical Coherence Tomography

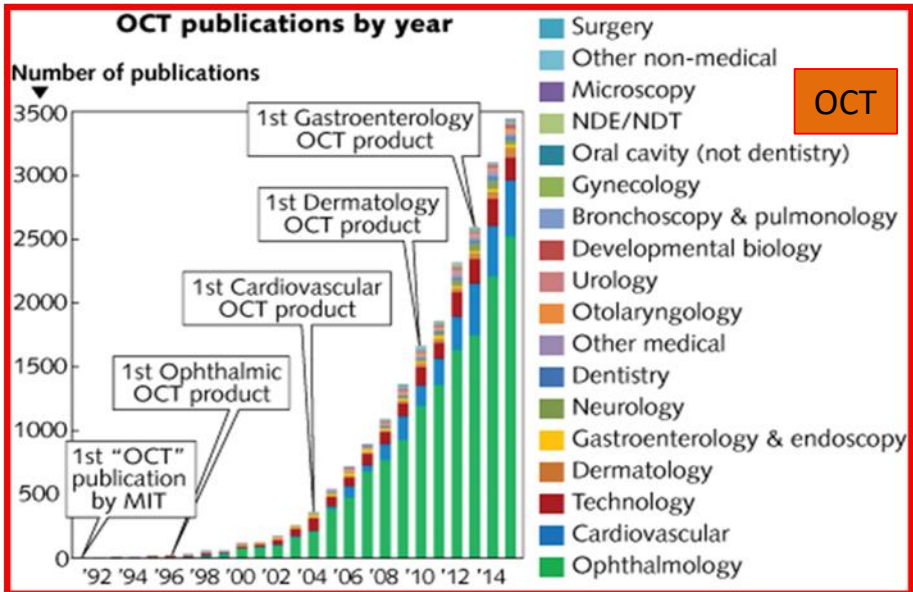
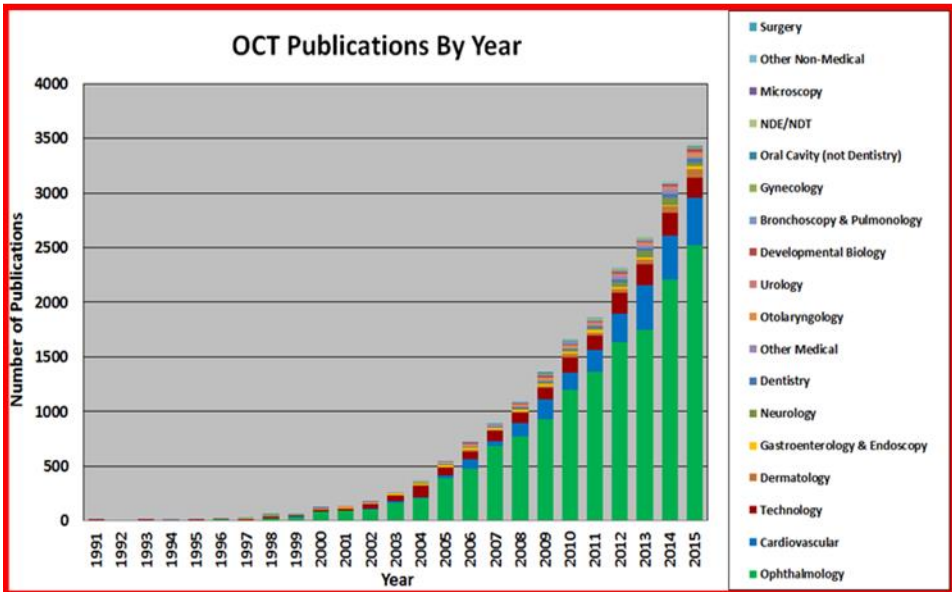
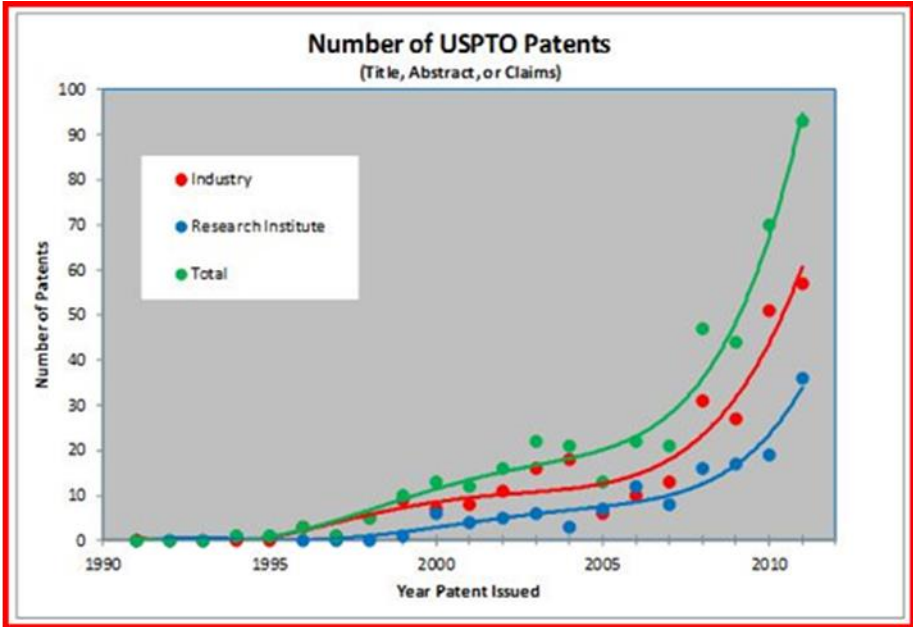
by: James Fujimoto and David Huang

9 12

**1B\$ = 10 ≠ 1B€ = 10**  
**Scale metriche ≠ dal 1974**

The market is just over \$1B in 2012, and it is expected to grow by 18–30% per year for the foreseeable future

±50.000 OCT/AngioOCT  
 ±250.000 Ophthalmologists



OCT



## A Method of Photographing Fluorescence in Circulating Blood in the Human Retina

By HAROLD R. NOVOTNY, B.S., AND DAVID L. ALVIS, M.D.

**T**HE PHYSIOPATHOLOGY of the retinal vasculature would be better understood if more were known about blood flow in these vessels. Because of the unique quality of transparency in the eye, methods depending on direct observation of the retinal vessels seem especially inviting. Already reported by various authors are techniques for

exciting wave length was 520 mμ, in the green. Kodak wratten filters no. 47 and no. 58, combined with a 3-mm. layer of 0.25 M copper sulfate, were accordingly inserted into the optical system (figs. 1 and 2) at appropriate points. In order to modify the activating light, the blue no. 47 filter was placed in the path of the beam from the electronic flash and from the incandescent viewing source. This made it possible to see, as well as to photograph, the fluorescence

*Image shows at the Fovea:*

2.0 x 2.0 mm (A)

3.0 x 3.0 mm (B)

6.0 x 6.0 mm (C)

8.0 x 8.0 mm (D)

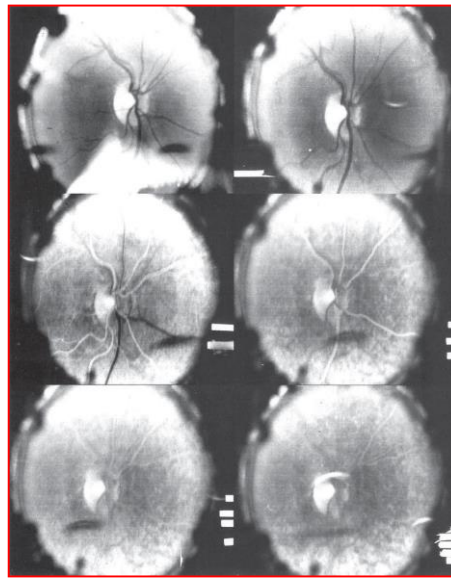
**12 x 12 mm 12 x 16 mm**

*Images at the Optic Nerve:*

3.0 x 3.0 mm (E)

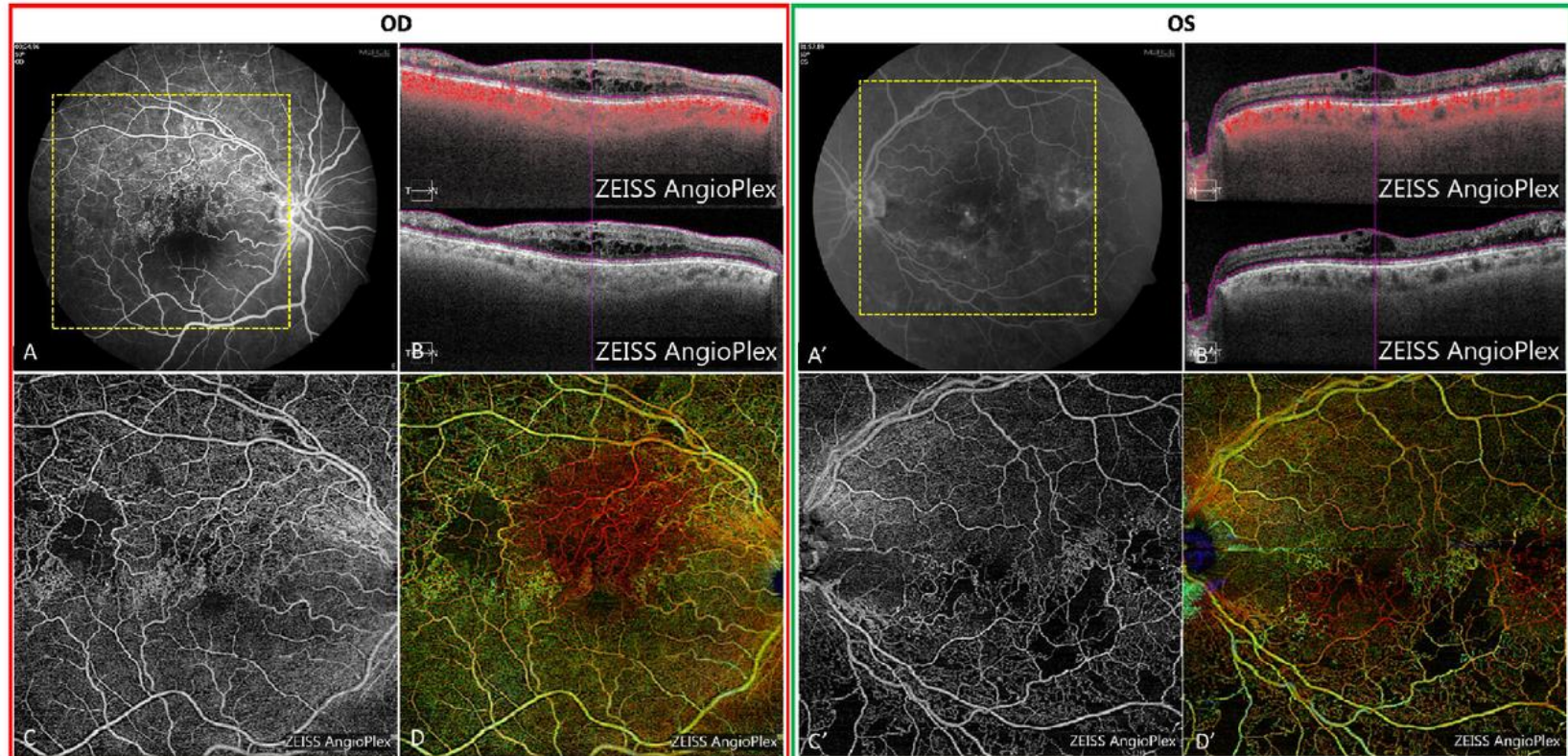
6.0 x 6.0 mm (F)

**8.0 x 8.0 mm**


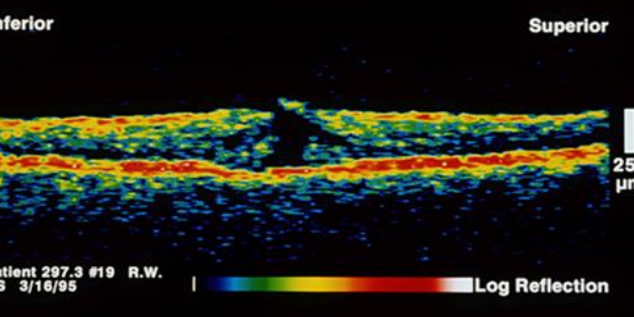

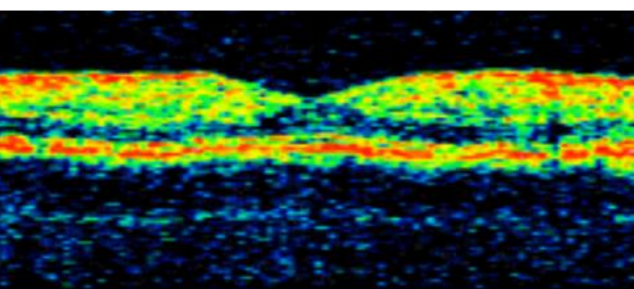

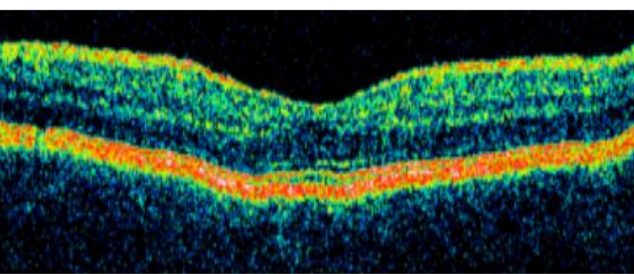

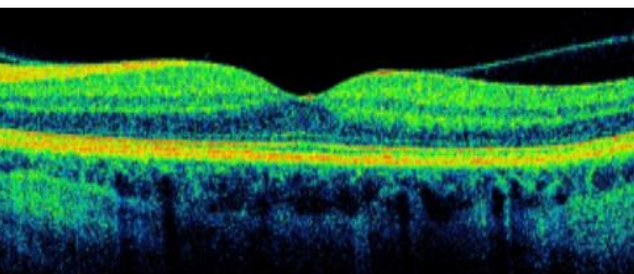


H. Novotny and D. Alvis; Circulation 1961

**The first fluorescein angiogram taken in November 1959, of the right eye of David Alvis with Harold R. Novotny**





Model Image	Year	Single line Scan	Scans Sec	Resolution (microns)	50000 OCT B Scan 250000 Ophthalmologists
	<div data-bbox="463 228 579 328" style="background-color: red; color: white; padding: 5px; text-align: center;">OCT 1995</div> <div data-bbox="444 342 579 399" style="border: 1px solid blue; padding: 2px;">200/99</div>	100 A-scans x 500 points	100	20	 <p>Inferior Superior</p> <p>250 μm</p> <p>Patient 297.3 #19 R.W. OS 3/16/95</p> <p>Log Reflection</p>
	<div data-bbox="463 514 579 614" style="background-color: red; color: white; padding: 5px; text-align: center;">OCT2 2000</div> <div data-bbox="425 628 579 685" style="border: 1px solid blue; padding: 2px;">400/2002</div>	100 A-scans x 500 points	100	20	
	<div data-bbox="444 785 598 913" style="background-color: red; color: white; padding: 5px; text-align: center;">OCT3 Stratus 2002</div> <div data-bbox="415 928 598 985" style="border: 1px solid blue; padding: 2px;">6000/2006</div>	512 A-scans x1024 points	500	10	
	<div data-bbox="444 1128 598 1256" style="background-color: red; color: white; padding: 5px; text-align: center;">Cirrus HD-OCT 2007</div> <div data-bbox="415 1285 598 1328" style="border: 1px solid blue; padding: 2px;">10000/2012</div>	4096 A-scans x 1024 points	27,000	5	

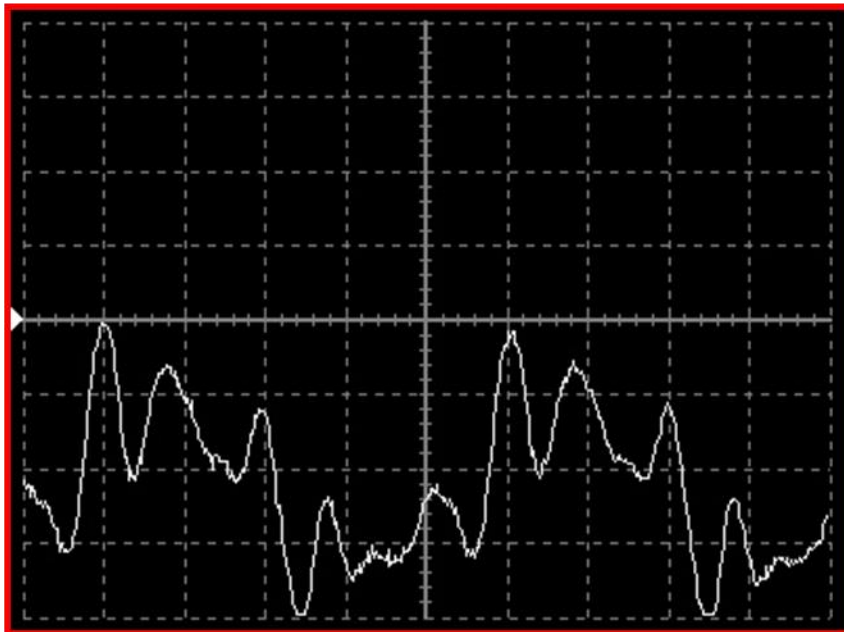
## Dawn of a New Era in Imaging

**$x(t)$  vs  $X(f)$**

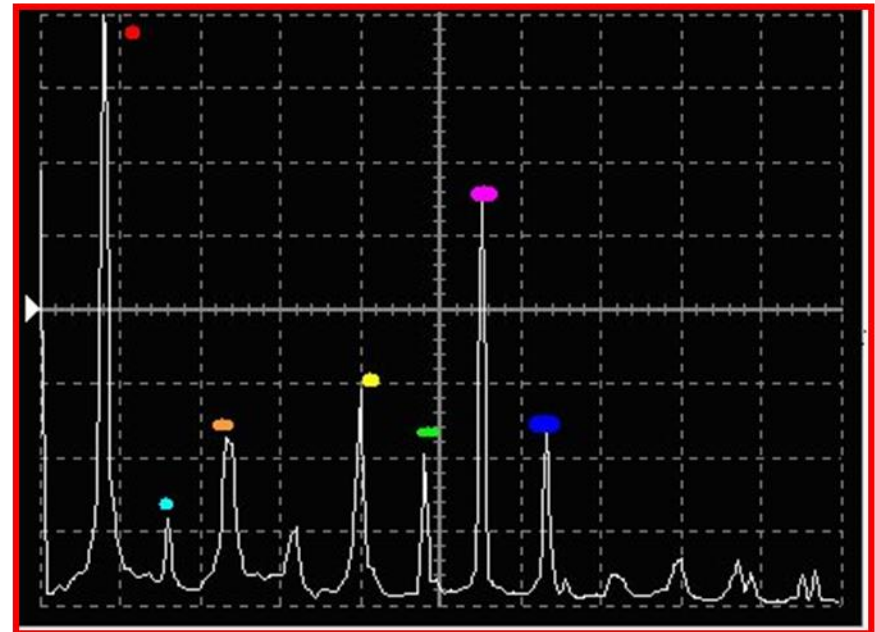
$$X(f) = \int_{-\infty}^{+\infty} x(t) \cdot e^{-j2\pi f t} dt$$

$$x(t) = \int_{-\infty}^{+\infty} X(f) \cdot e^{+j2\pi f t} df$$

## Trasformata e Antitrasformata di Fourier



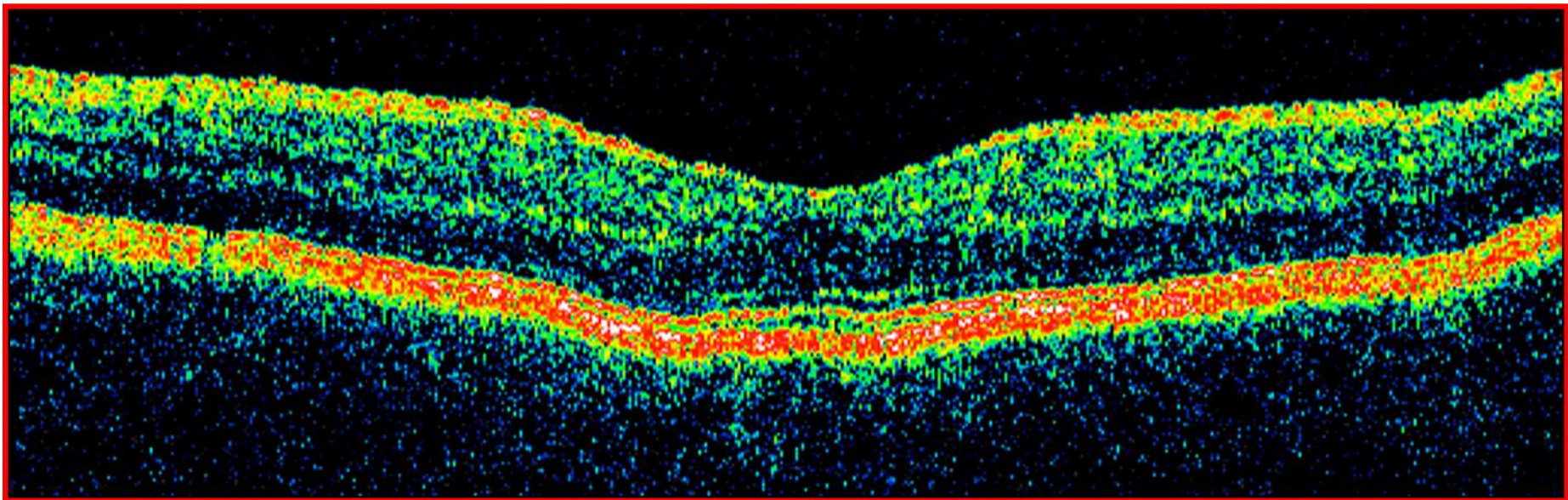
Nota musicale «**la**» di un clarinetto registrata tramite oscilloscopio nel dominio del tempo  **$x(t)$**



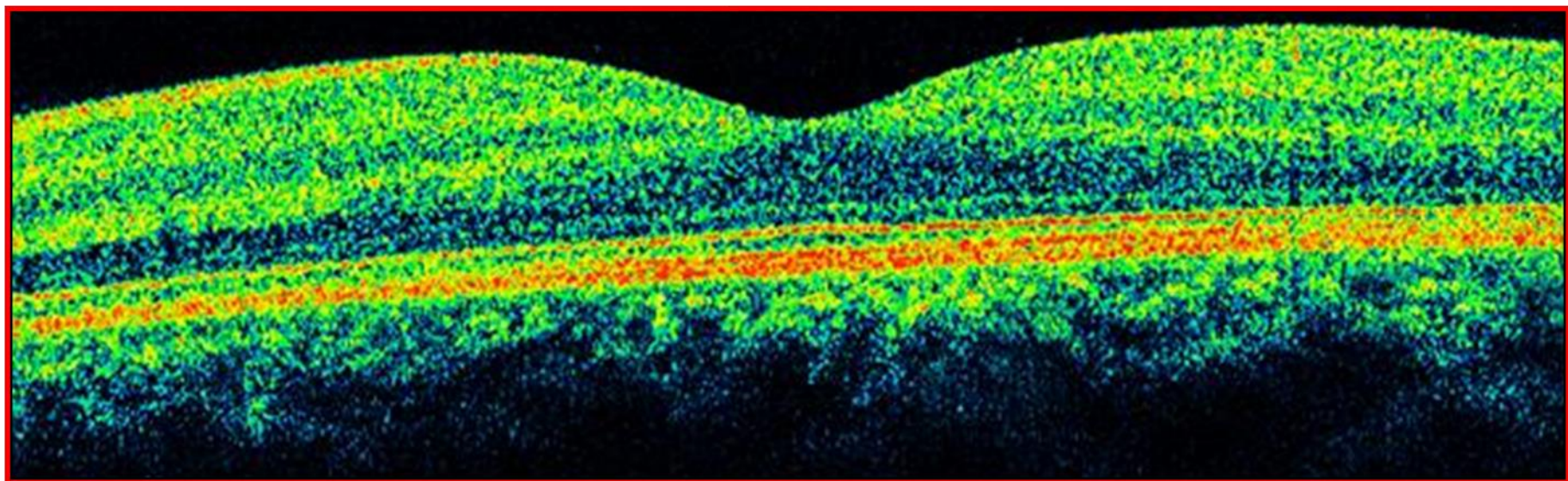
Nota musicale «**la**» di un clarinetto scomposta in sotto-onde nel dominio delle frequenze  **$X(f)$**



$x(t)$



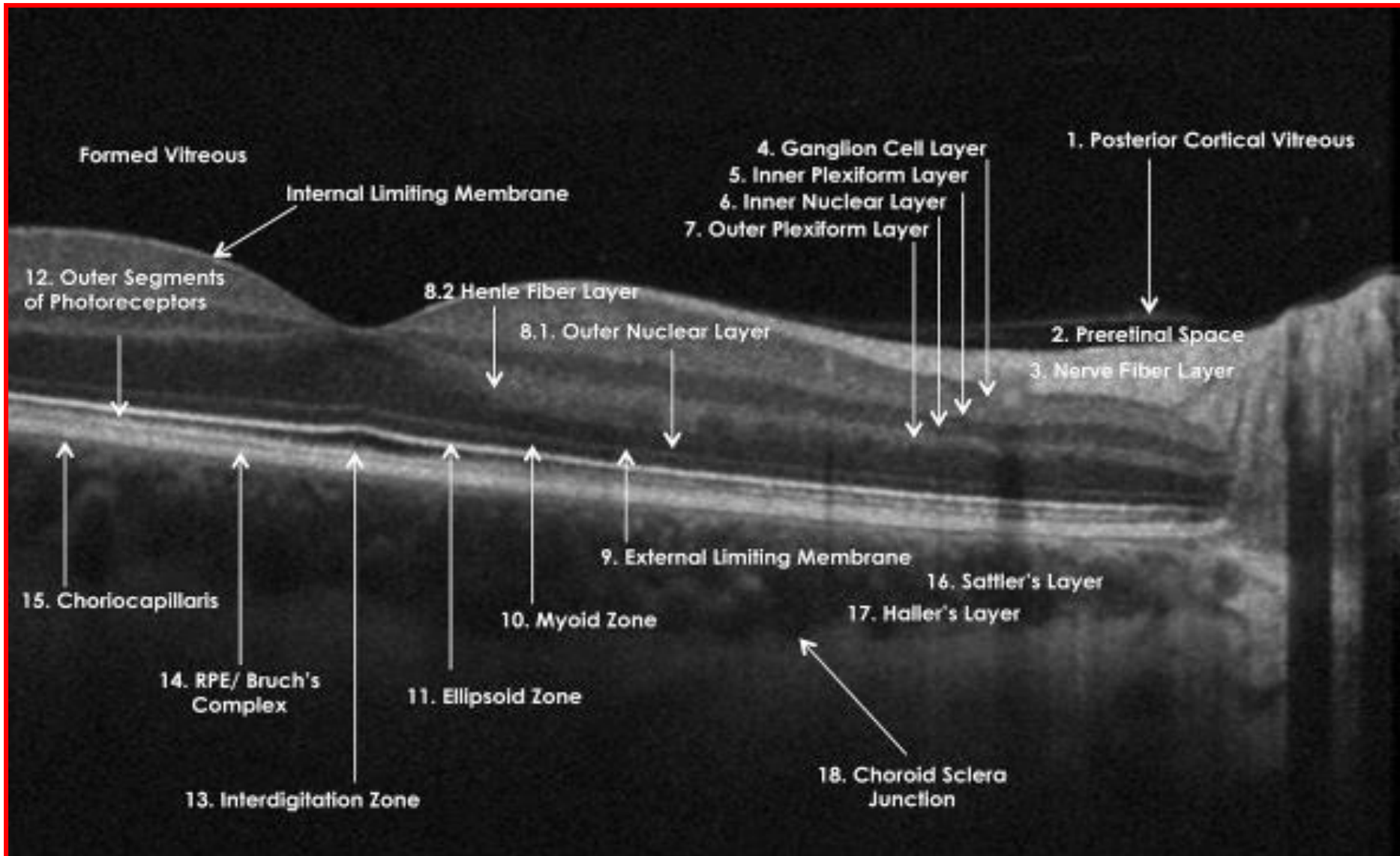
$x(f)$



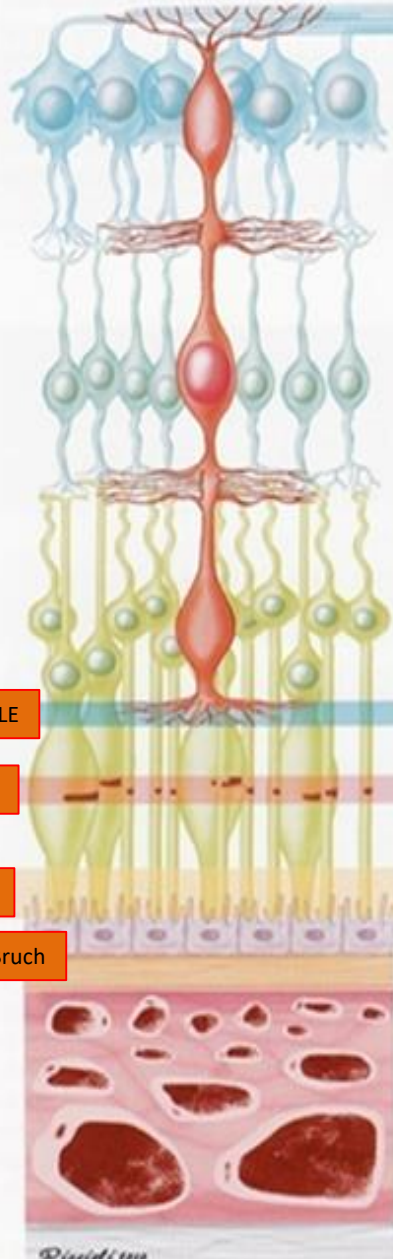


# International Nomenclature OCT (INOCT) 2014

By: Staurengi G, Sadda S, Chakravarthy U, Spaide RF; International Nomenclature for Optical Coherence Tomography (IN•OCT) Panel.



## Strati della retina e della coroide



MLE

EZ

IZ

EPR Bruch

Mioide

Si può osservare, dall'alto in basso, lo strato delle fibre del nervo ottico con la limitante interna formata da fibrille di cellule di Müller.

Strato delle cellule ganglionari, i cui assoni formano lo strato delle fibre ottiche.

Plessiforme interna, dove si connettono le cellule bipolari e ganglionari. Vi sono strutture orizzontali formate in parte da fibrille delle cellule di Müller.

Strato nucleare interno delle cellule bipolari.

Strato plessiforme esterno, dove si connettono fotorecettori e cellule bipolari. Sono presenti anche strutture orizzontali delle cellule orizzontali e fibrille delle cellule di Müller.

Strato dei nuclei dei fotorecettori.

La membrana della limitante esterna, formata da fibrille provenienti dalle fibre di Müller, forma una rete che circonda coni e bastoncelli.

Giunzione segmento interno e segmento esterno dei fotorecettori.

Segmento esterno dei coni e dei bastoncelli.

Giunzione fra estremità esterna dei coni e dei bastoncelli e fibrille delle cellule epiteliali.

Corpo delle cellule epiteliali.

Membrana di Bruch e coriocapillare.

Strato di Sattler dei piccoli vasi della coroide.

Strato di Haller dei grandi vasi della coroide.

Interfaccia fra coroide e sclera.

Sclera.

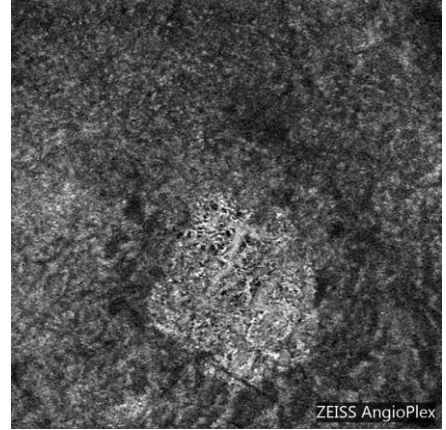
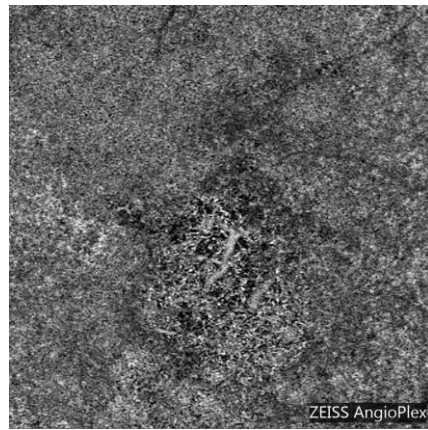
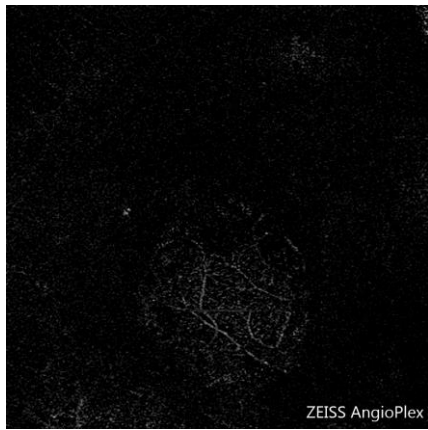
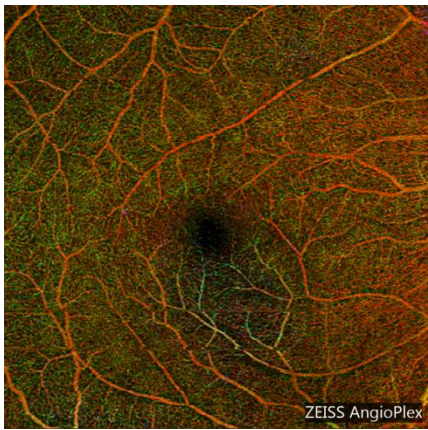
1) La membrana limitante esterna (**ELM**) si trova al confine tra i corpi cellulari (nuclei) e i segmenti interni dei fotorecettori e comprende gruppi di complessi giunzionali tra le cellule Müller e i fotorecettori.

2) La Zona Ellissoidale (**EZ**), precedentemente indicata come giunzione del segmento interno /segmento esterno del fotorecettore (**IS /OS**), è ora pensata per essere formata principalmente dai mitocondri all'interno dello strato ellissoidale della porzione esterna dei segmenti interni di i fotorecettori. In una fovea normale, la distanza dalla linea EZ all'ELM è inferiore a quella dalla linea EZ all'EPR

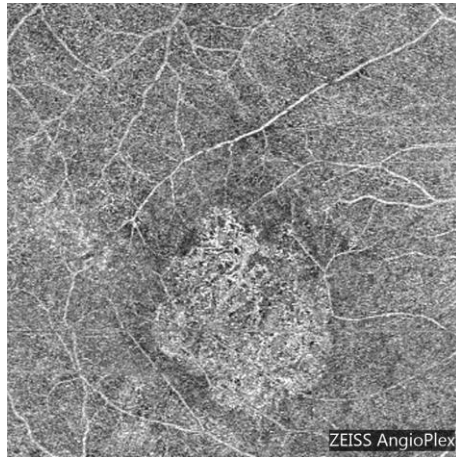
3) La Zona di Interdigitazione (**IZ**) corrisponde al cilindro di contatto rappresentato dagli apici delle celle EPR che racchiudono parte dei segmenti esterni del cono. Questo strato era precedentemente indicato come punte del segmento esterno del cono (**COST**) o punte del segmento esterno dello stelo (**ROST**), e non è sempre distinguibile dal livello RPE sottostante, anche nei soggetti normali.

4) La banda epiteliale del pigmento retinico è formata dall'EPR e dalla membrana di Bruch (indistinguibili l'una dall'altra in uno stato normale utilizzando gli attuali sistemi SD-OCT). Nella fovea, questa banda è più spessa, il che indica che le strutture coroidali possono anche contribuire all'iper-riflettività della banda RPE in questa posizione

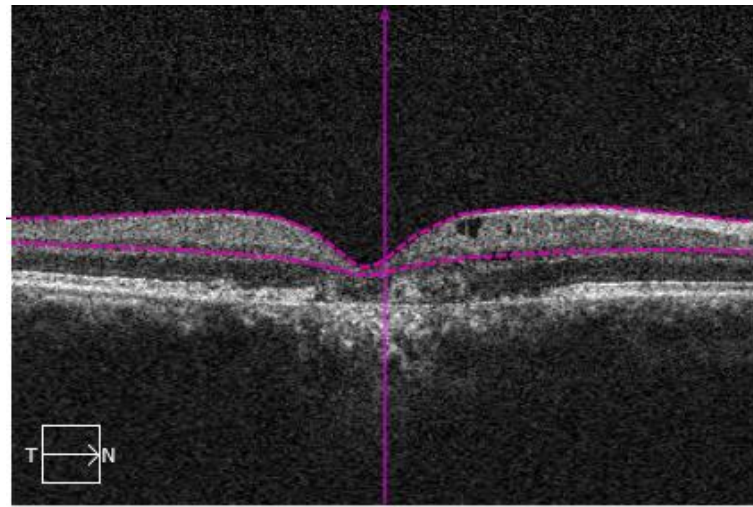
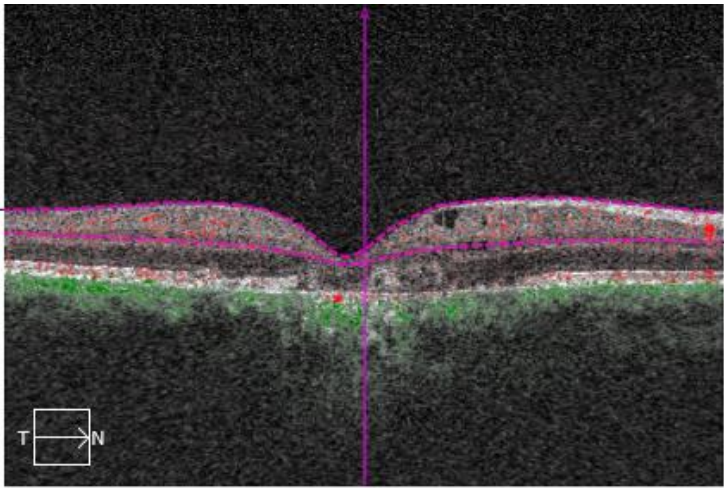




No Fovea EPR/EZ/IZ

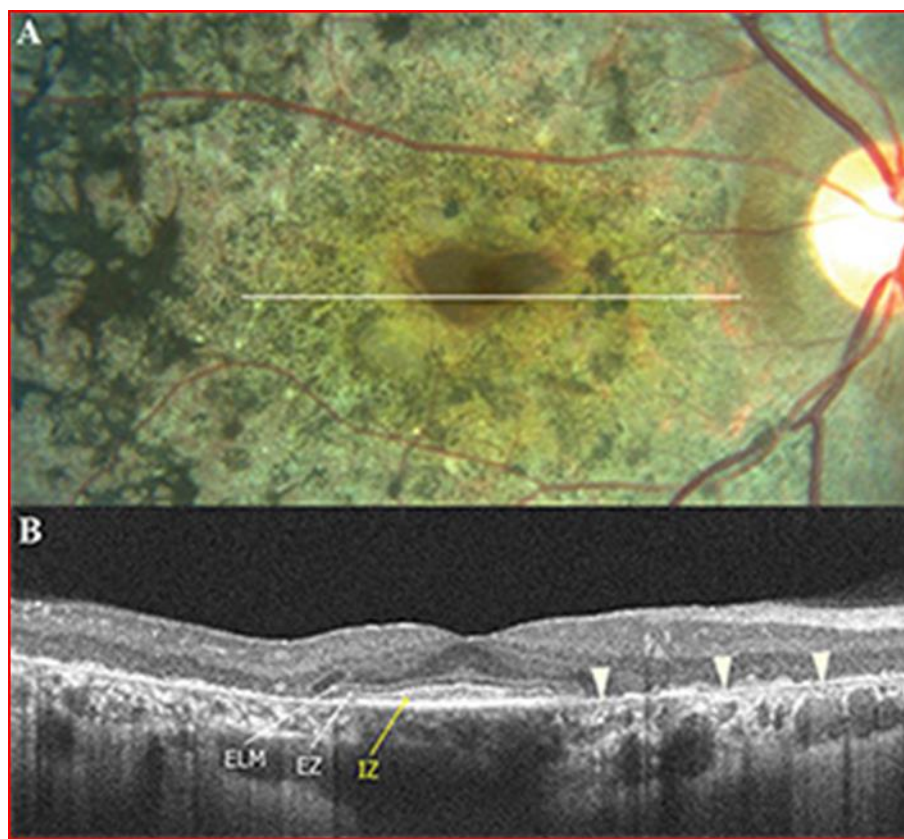


Low Visual Activity



However, OCT of retinal degenerative diseases over time has demonstrated that ELM, EZ and IZ lengths are highly correlated with each other, and disorganization seems to occur in a stepwise order: **first at the IZ**, followed by the EZ and finally the ELM line

The ELM zone has been reported as the first structure to recover after macular hole closure, and its recovery has been considered a sign of intact photoreceptor cell bodies and Müller cells



**“Outer Retinal Layers as Predictors of Vision Loss”** by  
**Marco A. Bonini Filho et al.**  
Published 15 April 2015



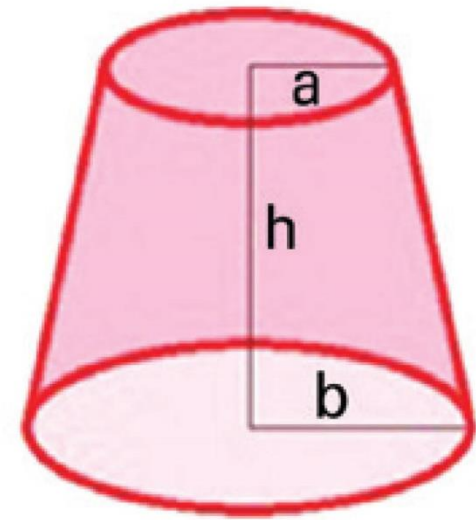
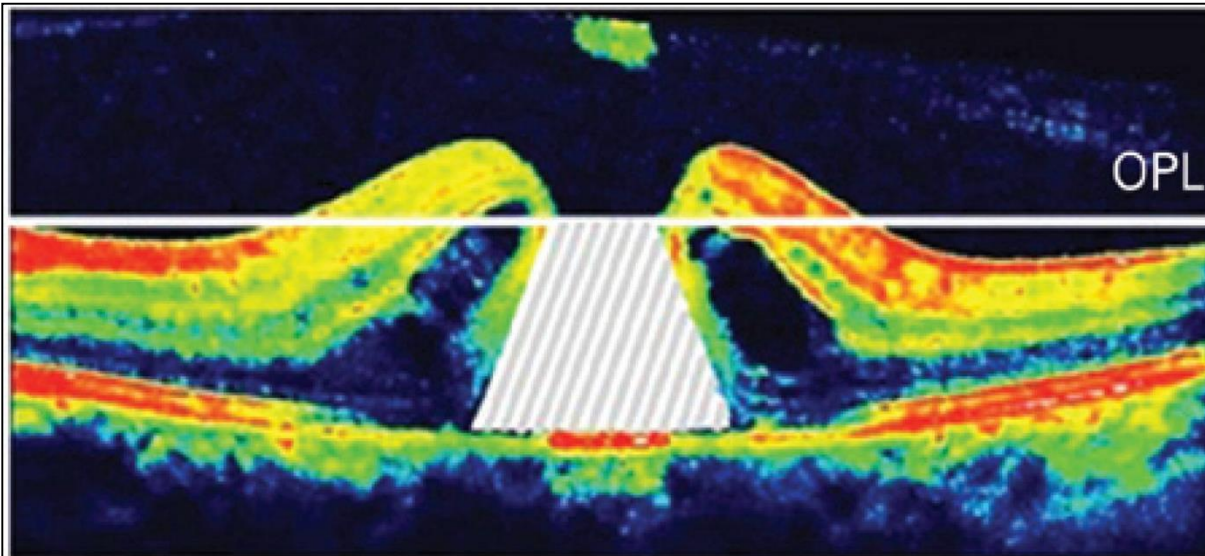
A relationship between the pre-treatment status of the ELM and post-treatment visual outcomes has been described for epiretinal membranes, age-related macular degeneration and diabetic macular edema.

Right eye of a 38-year-old woman diagnosed with retinitis pigmentosa. Best-corrected visual acuity was 20/30.

- A) The color photo showed typical pigment retinal epithelium atrophic abnormalities sparing the central macula.
- B) Spectral-domain optical coherence tomography showed that there was an extensive perifoveal region where outer retina layers (stars) were absent and the RPE was irregular or absent (arrowheads). However, the outer retinal bands were preserved in the foveal region, which correlated with the relatively normal visual acuity. Arrows indicate the end points of the **ELM, EZ and IZ, respectively**.



2  
+  
2  
≠  
4



$$V = \frac{\pi}{3} h (a^2 + ab + b^2)$$

**Calculation of the macular hole volume (MHV; mm<sup>3</sup>) according to the formula that gives the volume of a truncated cone**

by: Taylan Ozturk et al. Arq. Bras. Oftalmol. vol.79 no.3 **São Paulo May./June 2016**

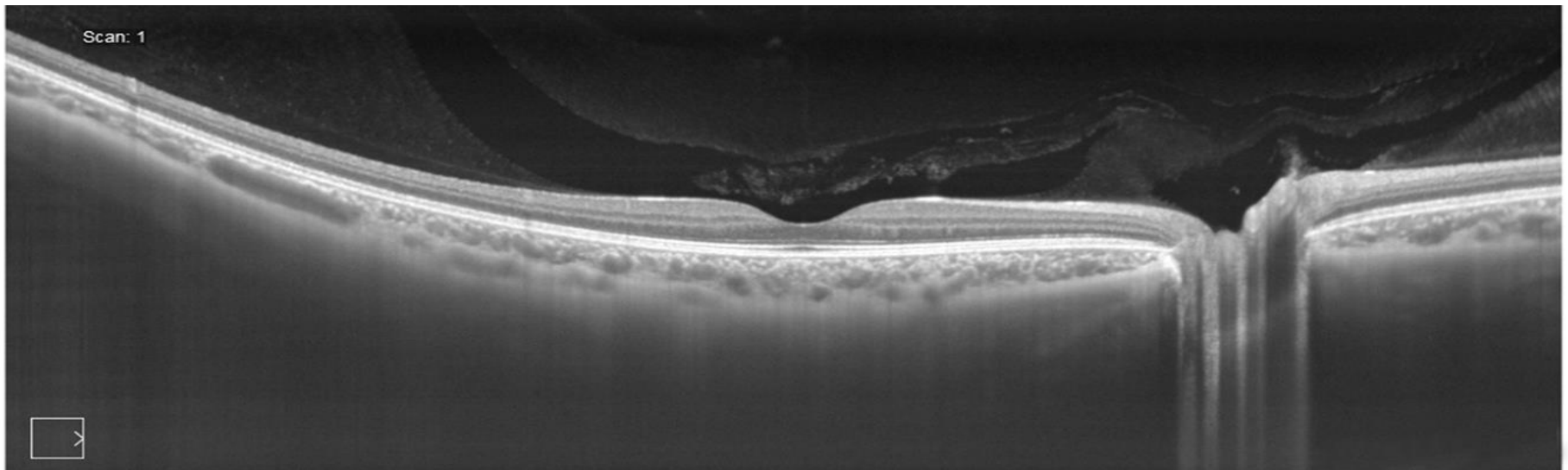
No statistical correlations were found between MHV and postoperative BCVA (p=0.588) and between MHV and disease recurrence (p=0.544). A weak negative correlation existed between MHV and final CMT (Central Macular Thickness) scores (p=0.04, r=-0.383).

Pre Retinal: Qualitative OCT Assessment  
Intra-Retinal: Qualitative OCT Assessment  
Sub-retinal/RPE: Qualitative OCT Assessment

- Pre-retinal membrane
- Epi-retinal membrane
- Vitreo-retinal strands
- Vitreo-retinal traction
- Syneresis
- Pre-retinal neovascular membrane NVE
- Pre-papillary neovascular membrane NVD

Diffuse intra-retinal oedema  
Cystoid macular oedema  
Hard exudate  
Scar tissue  
Atrophic degeneration  
Neovascularization

Choroidal neovascularization  
RPE detachment  
Drusen  
Sub-retinal fibrosis  
Scar tissue  
RPE atrophy



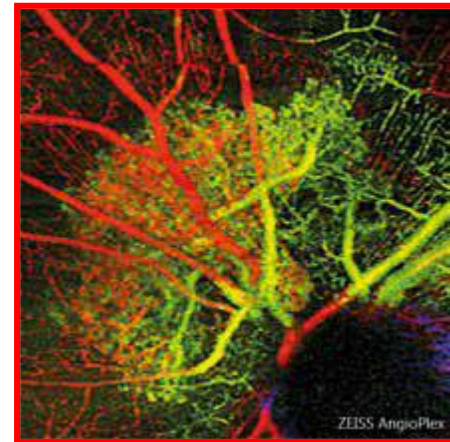
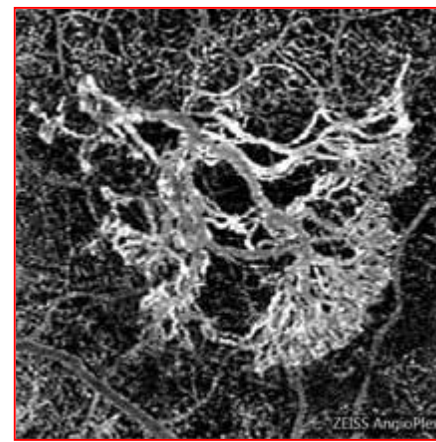
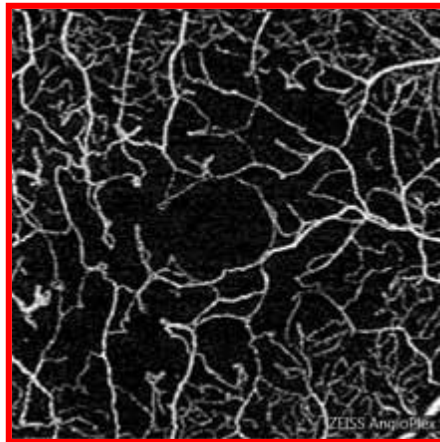
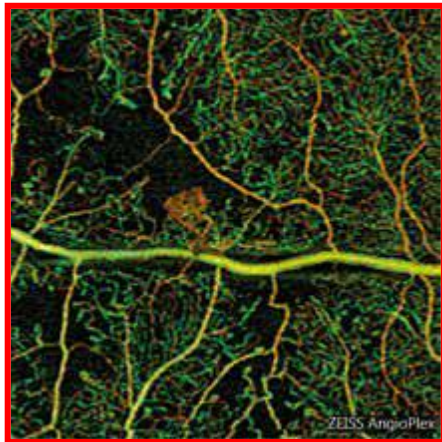
HD-Spotlight fino a 16 mm altamente dettagliato scansione B by SS-OCT Plex Elite Zeiss





ZEISS Academy Experience AngioPlex

**Dal segnale tomografico al segnale decorrelato: l'imaging vascolare nelle malattie neuroretiniche**



[www.amedeolucente.it](http://www.amedeolucente.it)



=

- 55,9% Zeiss **OCT**
- 35,6% Heidelberg By Mark Hillen
- 6,4% Topcon
- 2,1% Nidek

Mark Hillen. Benchmarking OCT. The Ophthalmologist, February 2016, #27

- Zeiss → **AngioPlex Cirrus 5000**
- Optovue → RTvue Avanti AngioVue
- Topcon → DRI OCT Triton
- Heidelberg → Spectralis con modulo OCT2
- Nidek → RS-3000 Advance OCT Angio-Scan
- Canon → OCT-HS100 Angio-eXpertcon modulo AX (Gruppo Haag-Streit)

- **HD-Cirrus Zeiss 68.000 A-Scan/Sec** → **OMAGc** (Optical Microangiography complex)
- RTvue Avanti Optovue 70.000 A-Scan/Sec → **SSADA** (Split Spectrum Amplitude Decorrelation Angiography)
- SS OCT DRI OCT Topcon 100.000 A-Scan/Sec → **OCTARA** (OCT Angiography Ratio Analysis)
- Spectralis Heidelberg 70.000 A-Scan/Sec → **Full SADA** (Spectrum Amplitude Decorrelation Algorithm)



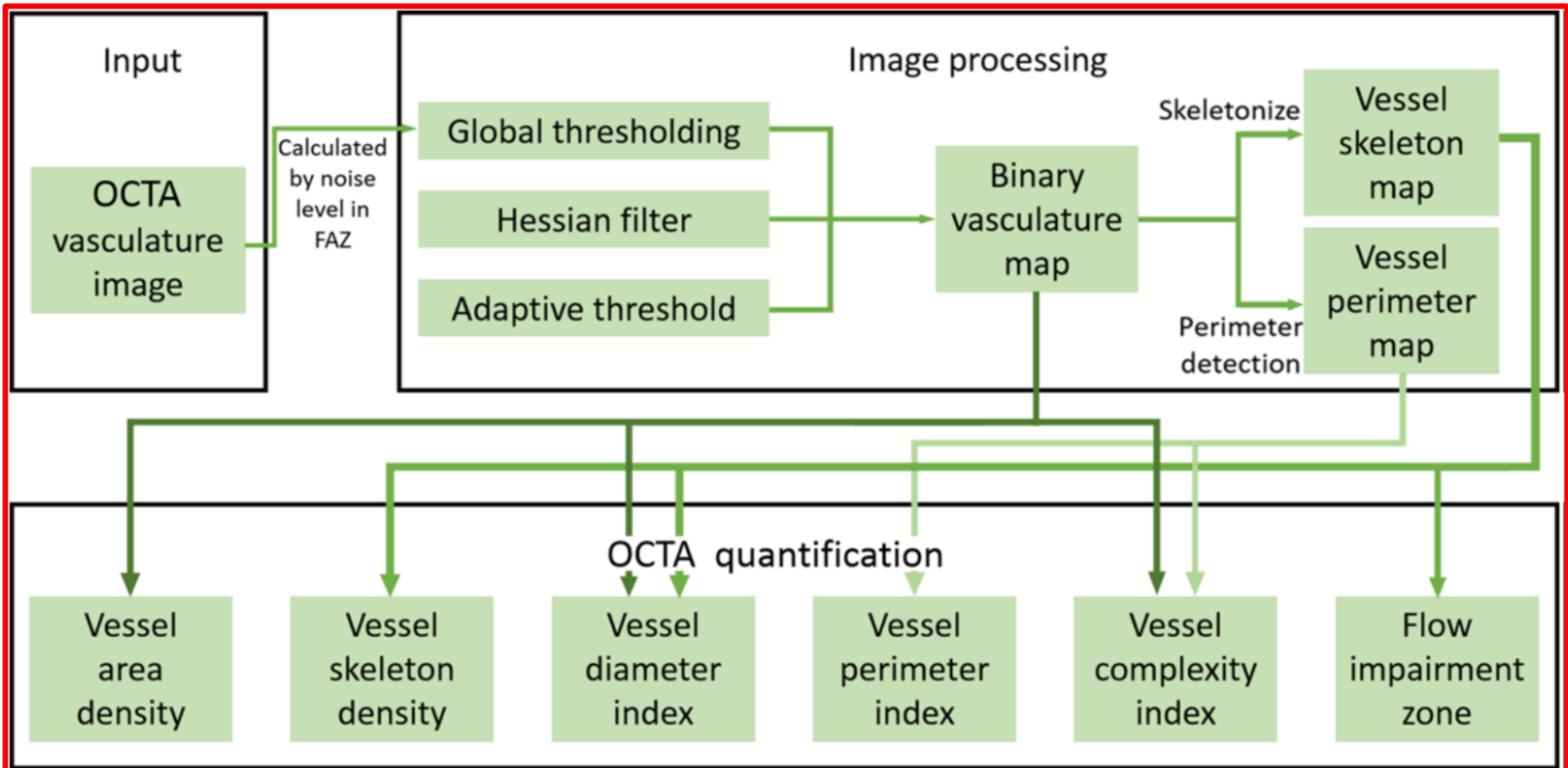
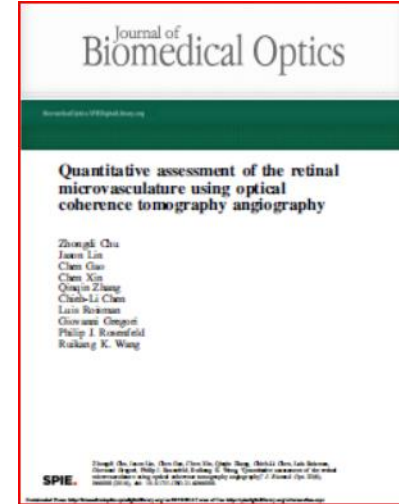
# Overview of the quantitative OMAG algorithm

vessel area density  
vessel skeleton density  
vessel diameter index  
vessel perimeter index  
vessel complexity index

Flowchart

MATLAB è un ambiente per il calcolo numerico e l'analisi statistica

by Zhongdi Chu et al. Journal of Biomedical Optics 21(6), 066008 (June 2016)



# The algorithms used in OCTA

- Optical microangiography (OMAG),
- Split-spectrum amplitude decorrelation angiography (SSADA)
- OCT angiography ratio analysis (OCTARA)
- Speckle variance
- Phase variance
- Correlation mapping.

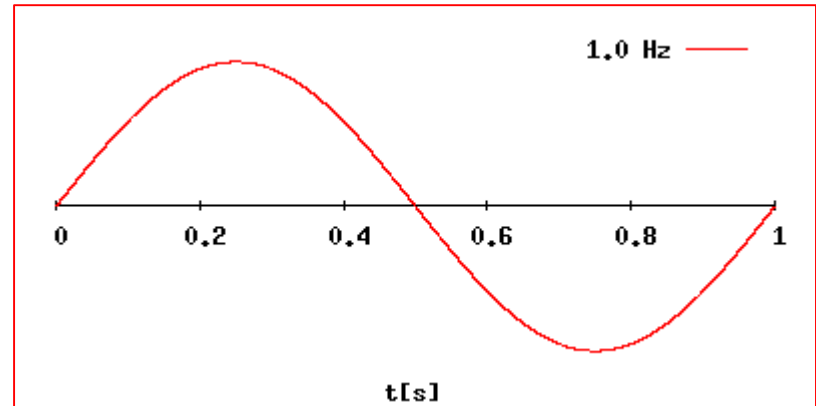
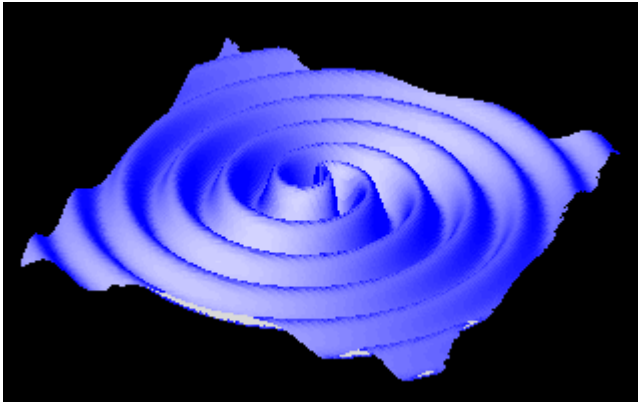
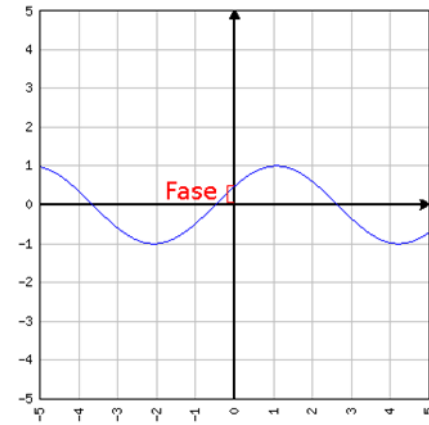
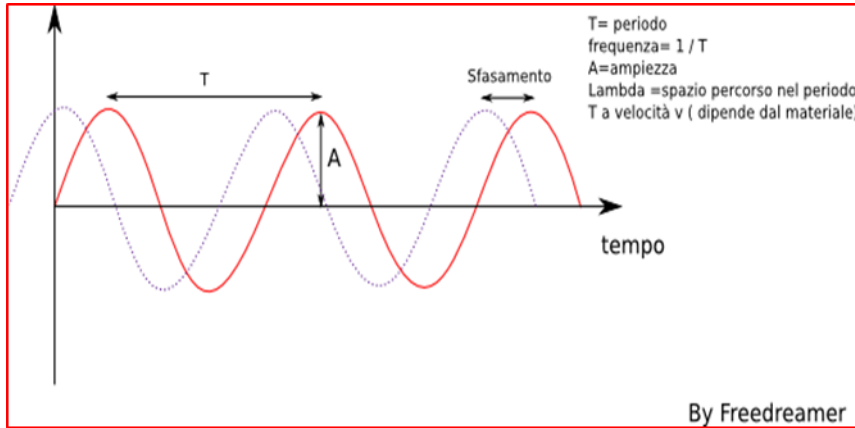
**Zhang A, Zhang Q, Chen CL, Wang RK**

Methods and algorithms for optical coherence tomography-based angiography: a review and comparison. J Biomed Opt. 2015 Oct;20(10):100901. doi: 10.1117/1.JBO.20.10.100901.

*In a recent study, when algorithms including OMAG, speckle variance, phase variance, SSADA and correlation mapping were compared, **it was found that OMAG**, as the method utilising complex OCT signals to contrast retinal blood flow **provided the best visual result for the of retinal microvascular networks concerning image contrast and vessel connectivity**.*



# What is a wave? «energy propagated through matter» A. Einstein



a) Angiografia dyeless basata sull'ampiezza del segnale OCT

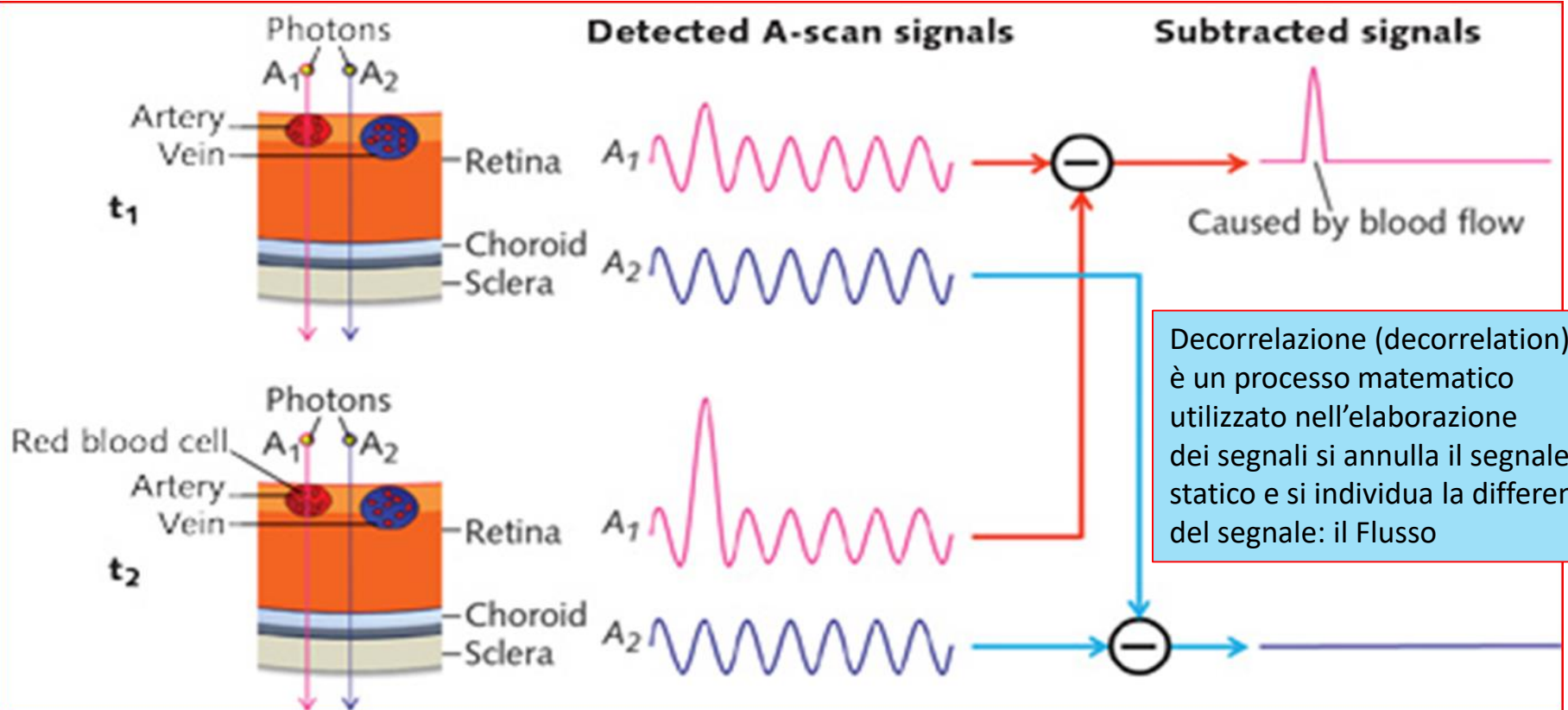
b) Angiografia dyeless basata sulla fase del segnale OCT

c) Angiografia dyeless basata sull'ampiezza e sulla fase del segnale OCT  
(complex signal)

# How OCTA Works



decorrelation

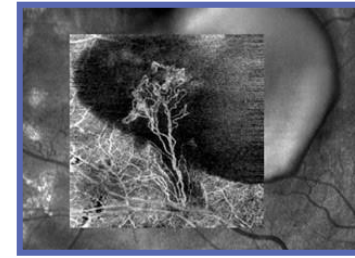


As moving blood cells pass through vessels, they generate changes in OCT signals. Based on this concept, a blood flow signal can be extracted by subtracting the OCT signals from the same location but at different time points (red path). The OCT signals will be different at these locations, while OCT signals from surrounding retinal tissues will remain steady (blue path).

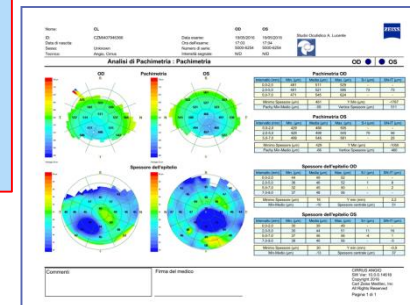
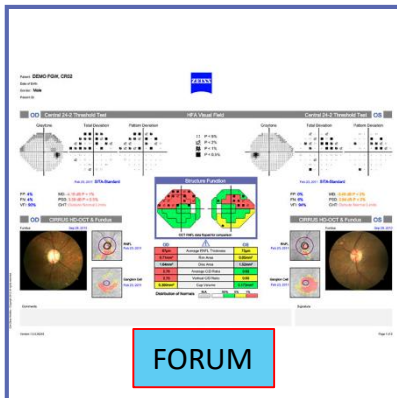
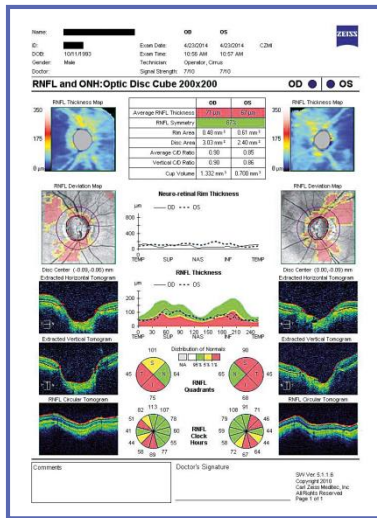
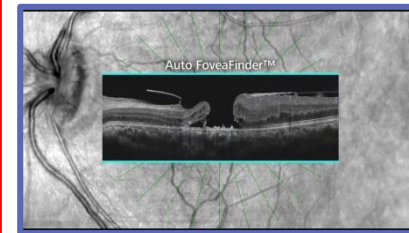
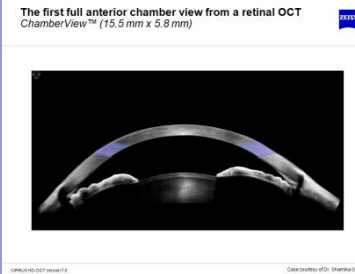
by **CHIEH-LI CHEN 11/13/2015 Bio Optics World**



# INDEX Angio Plex Cirrus



AngioPlex™ OCT  
 Angiography En face  
 Analysis Advanced RPE Analysis  
 Macular Thickness Analysis  
 Macular Change Analysis  
 HD 1 line  
 HD 21 Line  
 RNFL and ONH Analysis  
 ONH/RNFL Guided Progression Analysis™  
 (GPA™)  
 Ganglion Cell Analysis  
 GCA Guided Progression Analysis (GPA)  
 PanoMap™ Analysis  
 Anterior Chamber Analysis  
 Wide Angle-to-Angle  
 Analysis Pachymetry (epithelial and stromal thickness maps)  
 Analysis HD Cornea  
 HD Angle  
 HFA-CIRRUS Structure-Function Report



# Perfusion Density and Vessel Density

$$\text{Perfusion Density} = \frac{\text{Area Perfusa [mm}^2\text{]}}{\text{Area Totale [mm}^2\text{]}}$$

The flow index is defined as the average decorrelation values in the segmented area

$$\frac{\int_A D \cdot V dA}{\int_A dA} \quad \text{If not} \\ (V=1, \text{ if vessel; } V=0,$$

$$\text{Vessel Density [mm}^{-1}\text{]} = \frac{\text{Lunghezza Vasi [mm]}}{\text{Area Totale [mm}^2\text{]}}$$

The VD was defined as the percentage of signal-positive pixels/area of interest

The Vessel Density is defined as the percentage area occupied by vessels the segmented area

$$\frac{\int_A V dA}{\int_A dA} \quad \text{If not} \\ (V=1, \text{ if vessel; } V=0,$$

Numero di pubblicazione WO2014040070 A1

Tipo di pubblicazione Richiesta

Numero domanda PCT/US2013/059047

Data di pubblicazione 13 mar 2014

Data di registrazione 10 set 2013

Data di priorità 10 set 2012

Pubblicato anche come CA2883402A1, Altri 5 »

**Inventori David Huang, Yali Jia, Jason Tokayer, Ou Tan**

Candidato Oregon Health & Science University

Esporta citazione BiBTeX, EndNote, RefMan

Citazioni di brevetti (5), Con riferimenti in (1), Classificazioni (15), Eventi legali (4)



# Flusso Vessel Density

Nome:

ID: CZMI1545286560

Data di nascita:

Sesso: Unknown

Tecnico: Angio, Cirrus

Data esame:

Ora dell'esame:

Numero di serie:

Intensità segnale:

Precedente

08/06/2016

09:22

5000-6254

8/10

Corrente

26/04/2017

16:06

5000-6254

8/10

Studio Oculistico A. Lucente



## Analisi angiografica della variazione : Angiography 6x6 mm

OD ● ○ OS

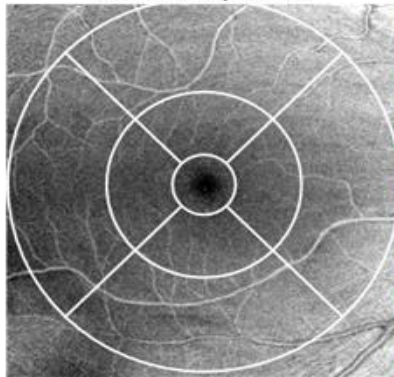
Esame 1 (scansione precedente)

08/06/2016 09:22:45

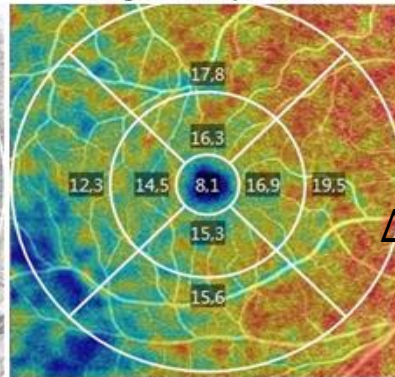
Segnale (8/10)



Struttura - Superficiale



AngioPlex - Superficiale



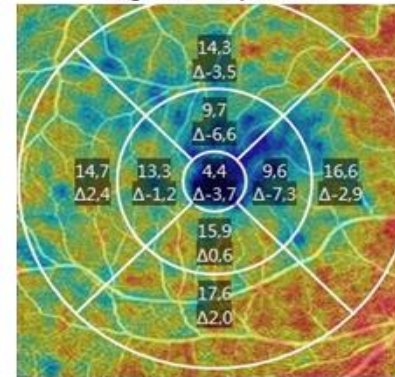
Segnale (8/10)



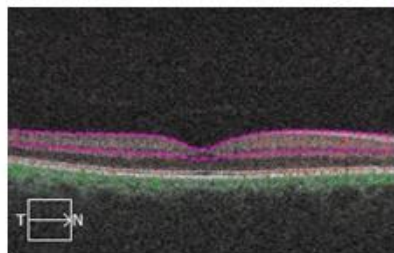
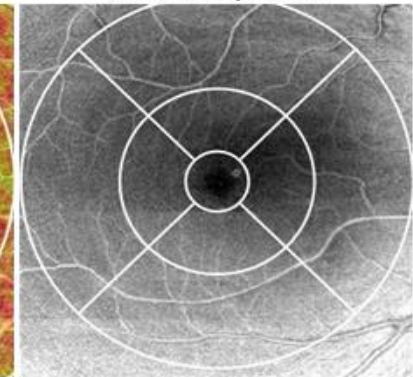
Esame 2 (scansione selezionata)

26/04/2017 16:06:15

AngioPlex - Superficiale



Struttura - Superficiale



Parte sup.: ILM Parte inf.: IPL  
Monitorato durante la scansione

Sovrapposizioni

Struttura - Nessuno  
AngioPlex - Vaso Mappa



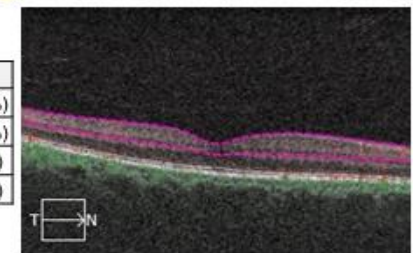
Angiometria

ETDRS - Vaso

Regione	Esame 1	Esame 2	Differenza
Centrale	8,1 mm <sup>-1</sup>	4,4 mm <sup>-1</sup>	-3,7 mm <sup>-1</sup> (-46%)
Interna	15,8 mm <sup>-1</sup>	12,1 mm <sup>-1</sup>	-3,7 mm <sup>-1</sup> (-23%)
Esterna	16,3 mm <sup>-1</sup>	15,8 mm <sup>-1</sup>	-0,5 mm <sup>-1</sup> (-3%)
Completo	16,0 mm <sup>-1</sup>	14,7 mm <sup>-1</sup>	-1,3 mm <sup>-1</sup> (-8%)

FAZ

	Esame 1	Esame 2	Differenza
Area	0,21 mm <sup>2</sup>	0,40 mm <sup>2</sup>	0,19 mm <sup>2</sup> (90%)
Perimetro	2,02 mm	3,60 mm	1,58 mm (78%)
Circularità	0,66	0,39	-0,27 (-41%)



Parte sup.: ILM Parte inf.: IPL  
Monitorato durante la scansione

Commenti

Firma del medico

# AngioPlex Metrix™ for HD-Cirrus 5000

- **Density measure (ETDRS, central, inner, full)**

densità dei vasi/Vessel Density

densità di perfusione/Flow Index

- **FAZ Parameters**

Area mm<sup>2</sup>

Perimetro (mm)

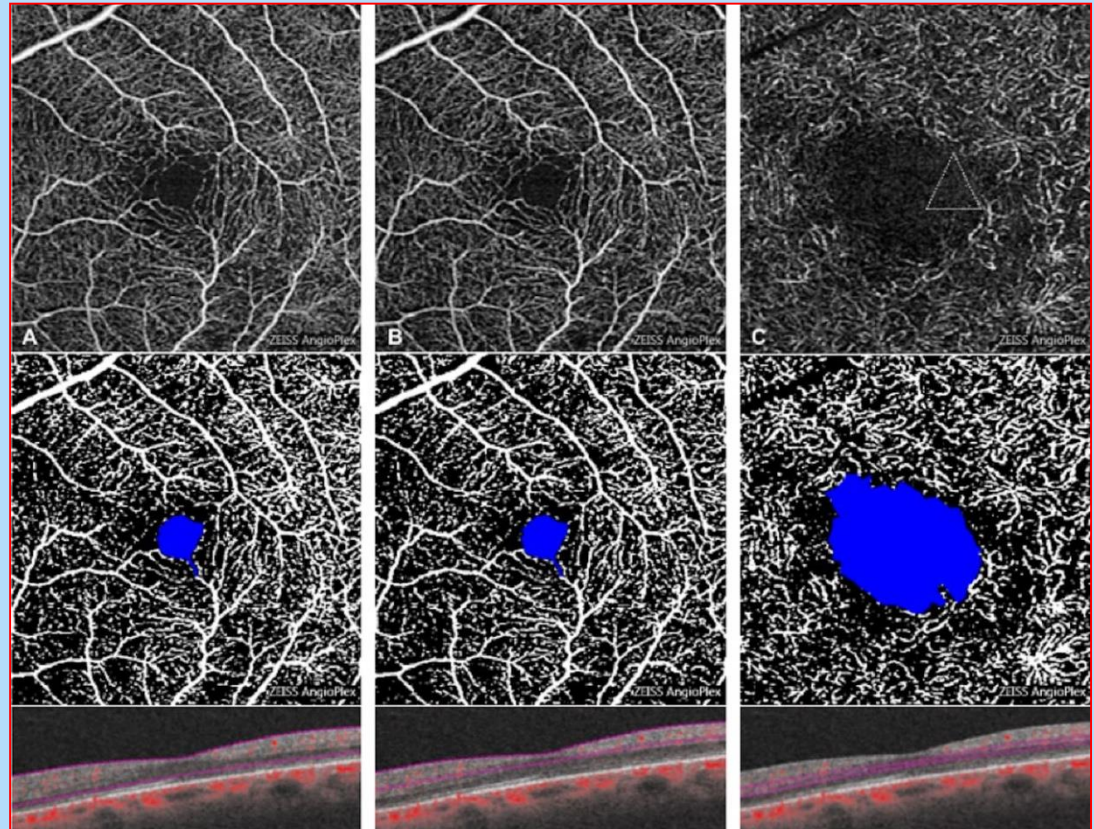
Circolarità della FAZ

- **Angiography Change**

Vessel Density

Fow Index

FAZ



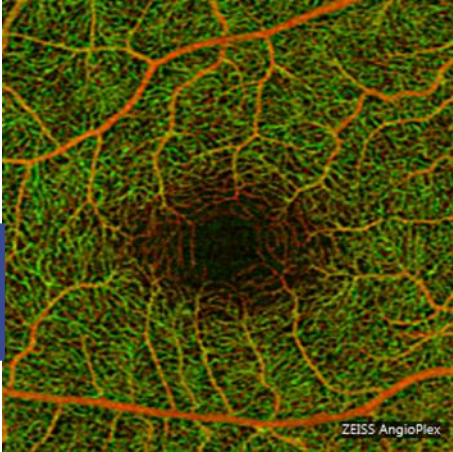
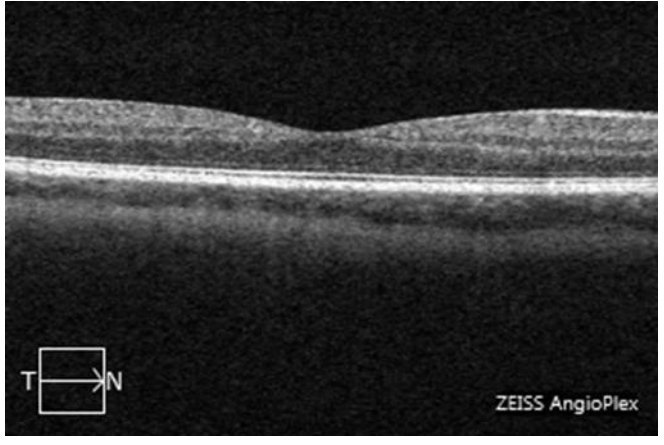
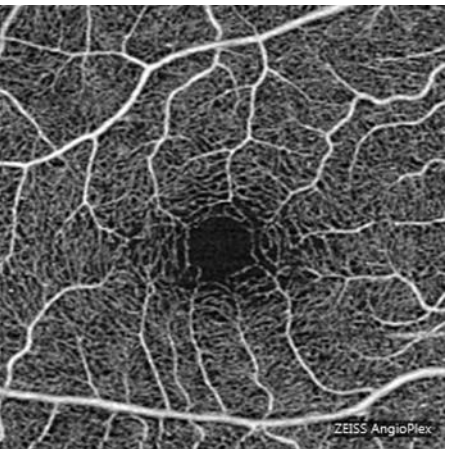
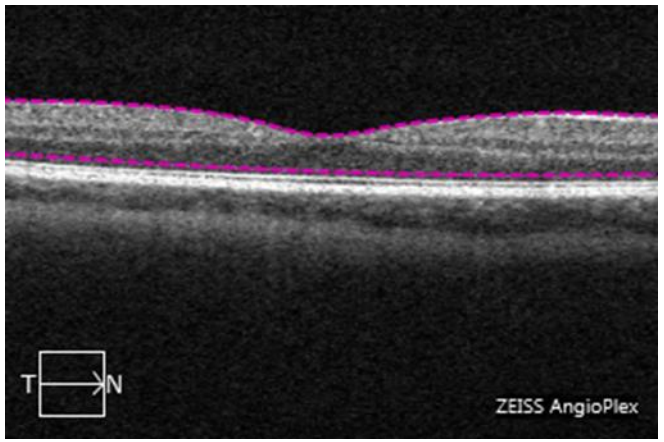


# AngioPlex & Analysis Layer

- 9slab +

Retina Encoded  
Retina  
VRI Vitreo-Retinal Interface  
Superficial Retinal Layer  
Deep Retinal Layer  
Avascular  
Choriocapillaris  
Choroid  
Occhio intero

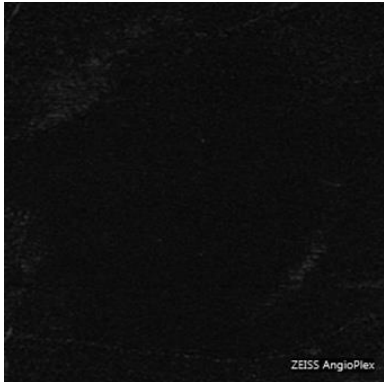
# AngioPlex Analysis Layer Presets: Retina Depth Encoded and Retina

Layer Preset	Layer Boundaries	Example Image (Normal Eye)	B-scan with Layers
<b>Retina Depth Encoded</b>	Combination of: Superficial, Deep, and Avascular Layers  Superficial: Red <b>S</b> Deep: Green <b>D</b> Avascular: Blue <b>A</b>	 <p style="text-align: right; font-size: small;">ZEISS AngioPlex</p>	 <p style="text-align: right; font-size: small;">ZEISS AngioPlex</p>
<b>Retina</b>	Inner Boundary: ILM  Outer Boundary: RPE = RPEfit - 70µm	 <p style="text-align: right; font-size: small;">ZEISS AngioPlex</p>	 <p style="text-align: right; font-size: small;">ZEISS AngioPlex</p>

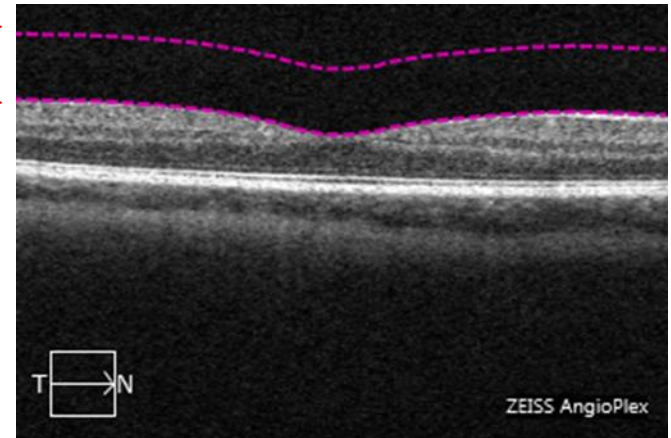


# AngioPlex Analysis Layer Presets: VRI and Superficial

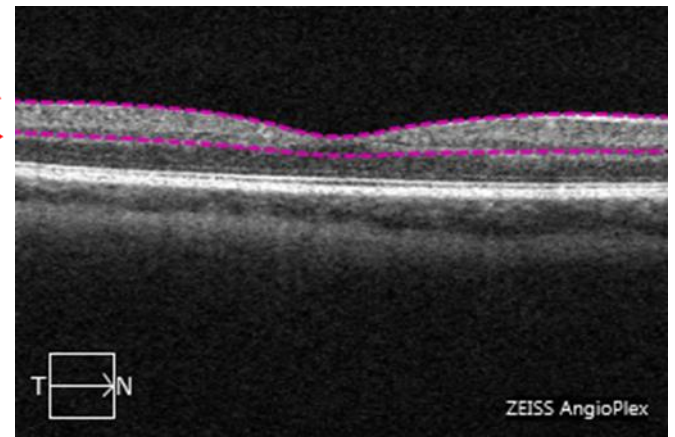
## - VRI Vitreo-Retinal Interface



Inner Boundary  
Outer Boundary ILM  
- 300µm



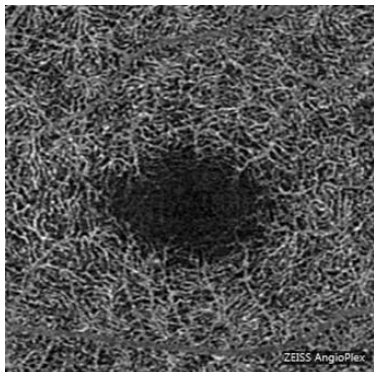
Inner Boundary ILM  
IPL=ILM+70%(OPL-ILM)  
Outer Boundary IPL



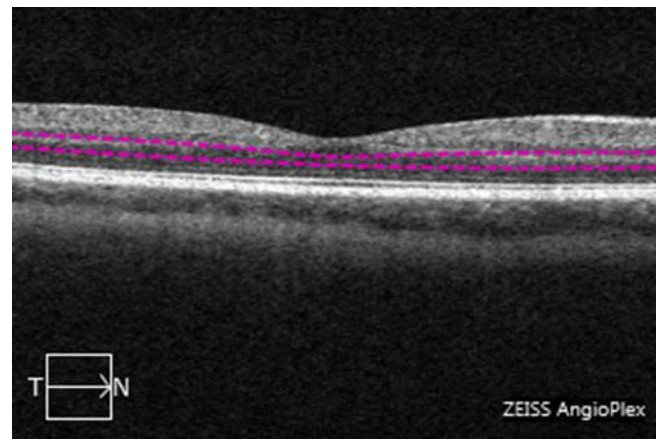
## - Superficial Superficial Retinal Layer

# AngioPlex Analysis Layer Presets: Deep and Avascular

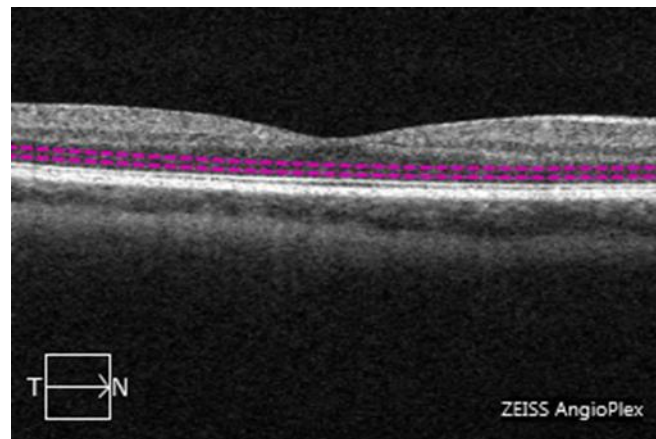
## - Deep Deep Retinal Layer



Inner Boundary IPL  
Outer Boundary OPL=RPEfit-110 $\mu$ m



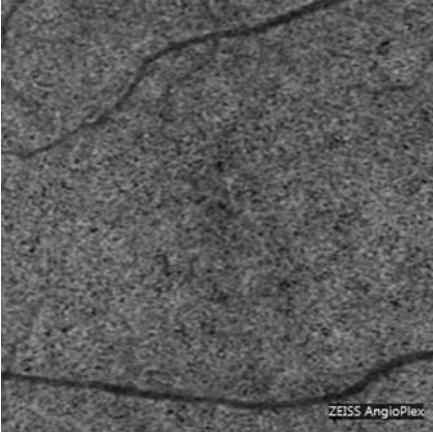
Inner Boundary OPL  
Outer Boundary IS/OS=RPEfit-70 $\mu$ m



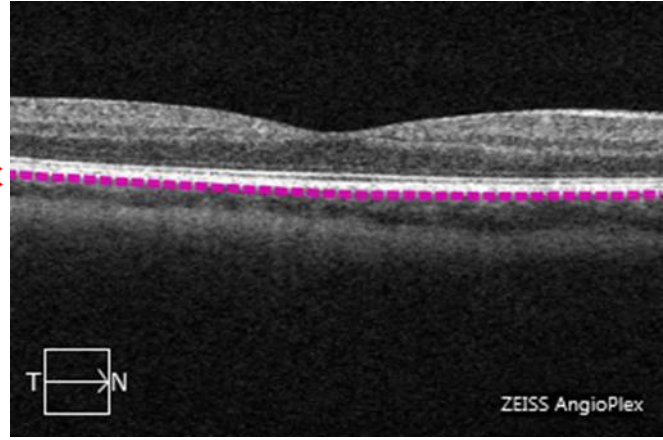
## - Avascular Avascular Retina

# AngioPlex Analysis Layer Presets: Choriocapillaris and Choroid

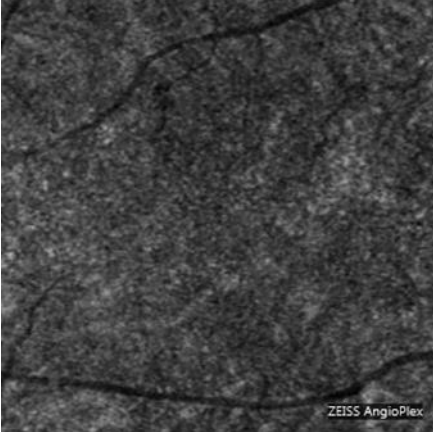
## - Choriocapillaris



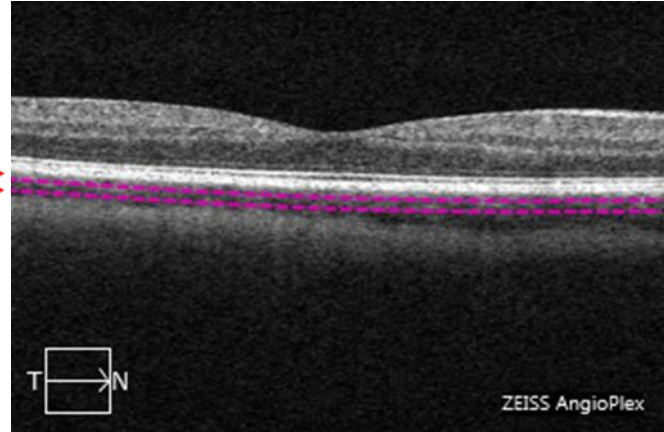
Inner Boundary CCIB=RPE+29 $\mu$ m  
Outer Boundary CCOB = RPE+49 $\mu$ m



## - Choroid



Inner Boundary ChIB = RPEfit + 64 $\mu$ m  
Outer Boundary ChOB = RPEfit + 115 $\mu$ m







# Thank you for your kind attention!

**Angio-Plex Cirrus HD Zeiss Über Alles**



[www.amedeolucente.it](http://www.amedeolucente.it)